

Numerical Simulations for the Planning of Surgical Procedures

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Why pediatric cardiac surgery?

How many people in the United States and in Europe have a congenital heart defect?

Estimates suggest that about 1,000,000 Americans have a congenital heart defect (American Heart Association). Approximately 36,000 babies are live born with a heart defect each year in the European Union (EUROCAT Central Registry).

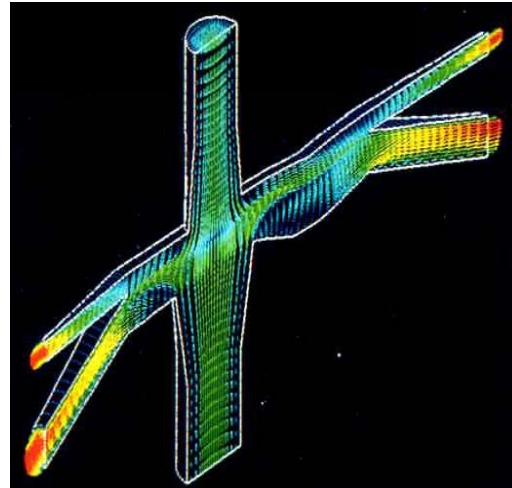
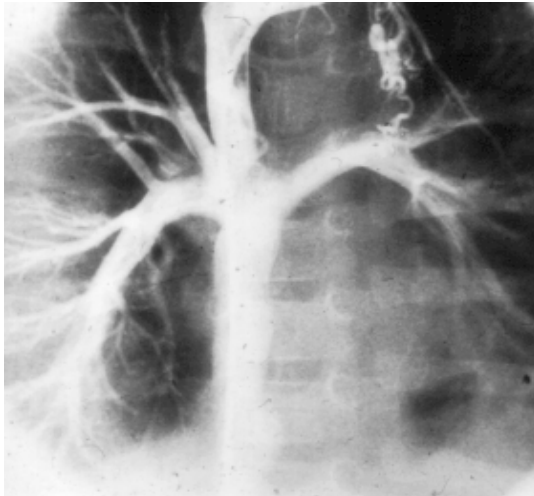
How serious is the problem?

Congenital heart defects are the most common birth defect and are the number one cause of death from birth defects during the first year of life. Nearly twice as many children die from congenital heart disease in the United States each year as die from all forms of childhood cancers combined. Over 91,000 life years are lost each year in the US due to congenital heart disease. Charges for care exceed 2.2 billion dollars, for inpatient surgery alone (American Heart Association).

Are things improving?

Definitely. Overall mortality has significantly declined over the past few decades. For example, in the 1960s and 1970s the risk of dying following congenital heart surgery was about 30% and today it is around 5%.

How the story started: back to Great Ormond Street Hospital for Children, London, 1993, and to the Total CavoPulmonary Connection (TCPC)



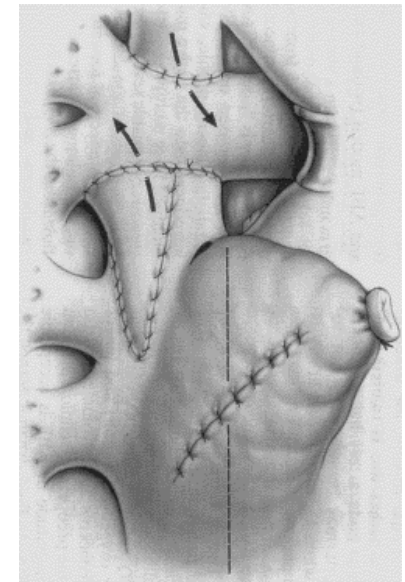
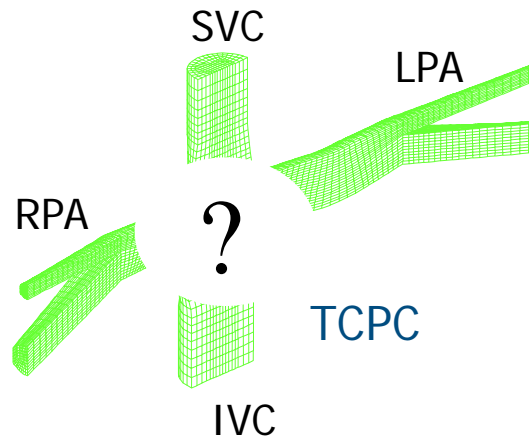
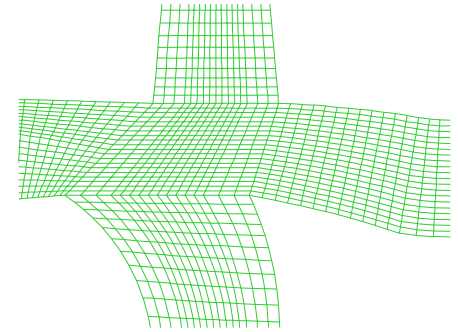
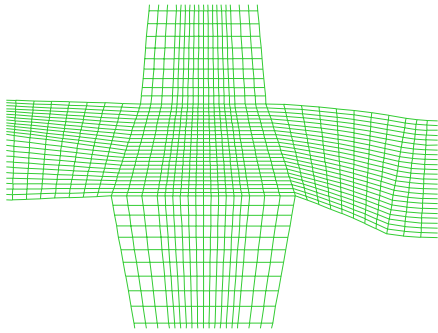
Prof. Marc R. de Leval
*Laurea ad honorem in
Biomedical Engineering,
Politecnico di Milano,
2007*

Aim:

To investigate the effects of geometric/anatomic features (e.g. *offsetting* and shape of the anastomosis between the inferior vena cava and the pulmonary artery)

de Leval et al. Use of computational fluid dynamics in the design of surgical procedures: application to the study of competitive flows in cavo-pulmonary connections, J Thorac Cardiovasc Surg. 1996

- 3-D geometry
- steady flow
- Newtonian fluid (*blood*)
- rigid walls



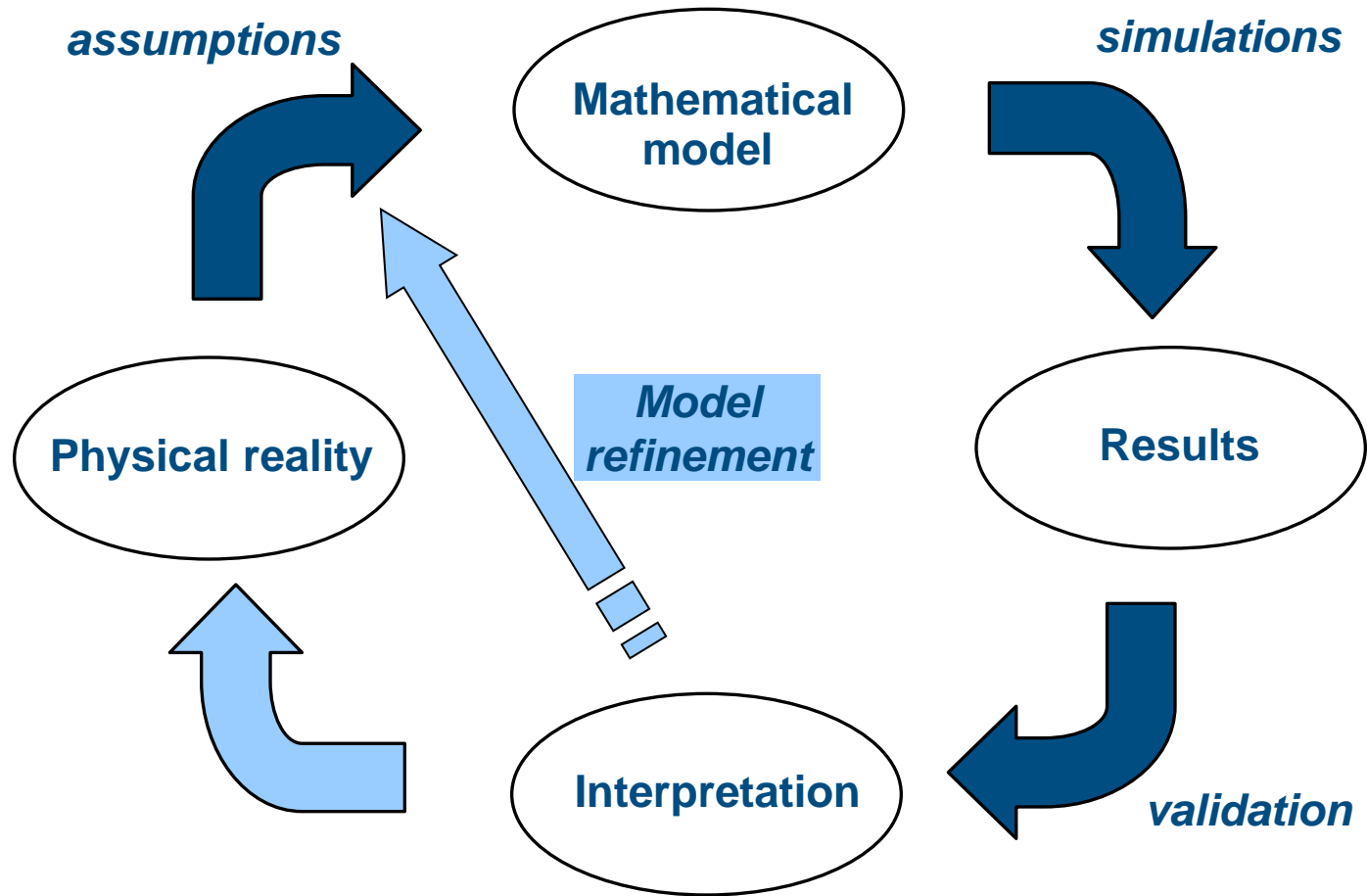
(de Leval et al., *J Thorac Cardiovasc Surg*, 96:682-695, 1988)

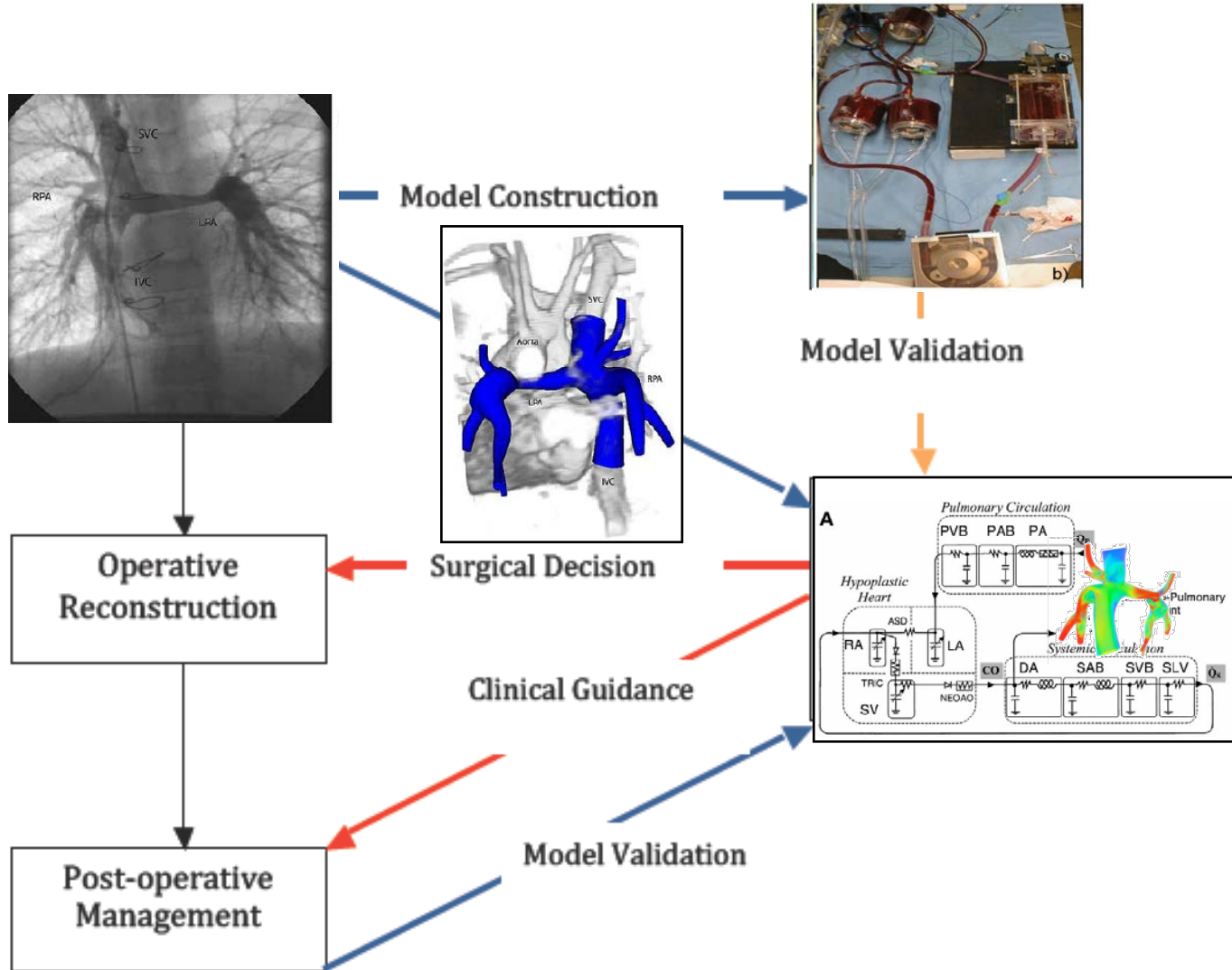
(de Leval et al., *J Thorac Cardiovasc Surg*, 113:502-13, 1996)

Numerical simulation for pediatric cardiac surgery:

1. To investigate phenomena hardly measurable in the clinical setting
 - energy dissipation (recirculation areas, jets, etc.)
 - blood and oxygen flow distribution to organs
2. To optimize the surgery technique
3. To plan surgery

- observations
- data





Computational Fluid Dynamics (CFD)

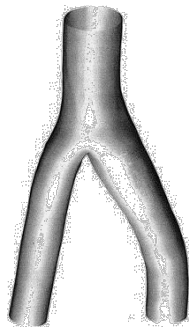
3D modelling

- local haemodynamics information
- rigid or deformable walls
- from idealized to patient-specific

accuracy
CPU time



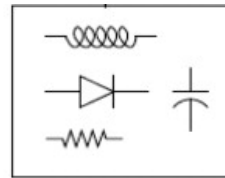
3D



1D



0D



R L C

1D modelling

- pulse wave propagation phenomena (curvature, branching, stenoses)
- rigid or elastic

0D modelling

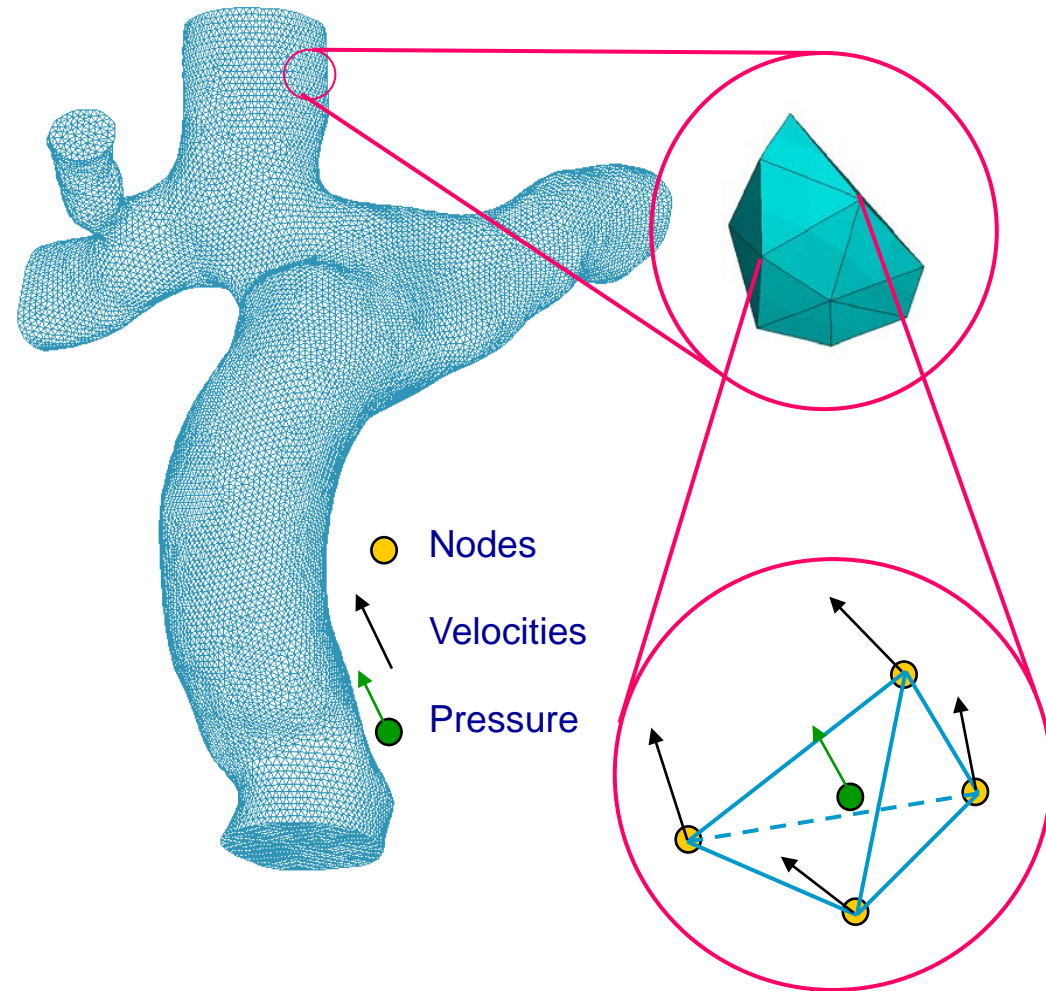
(lumped parameter, LPM)

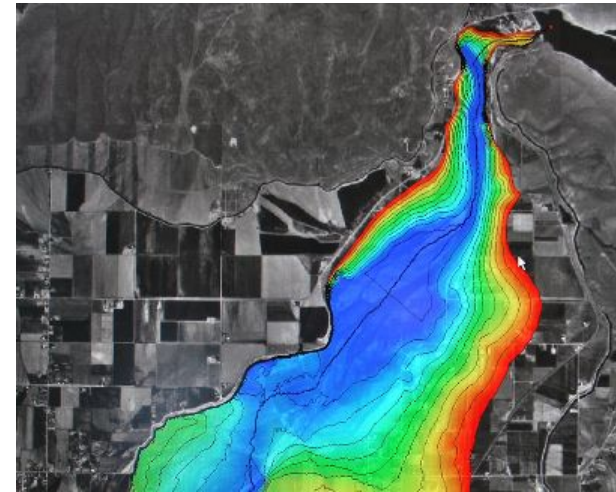
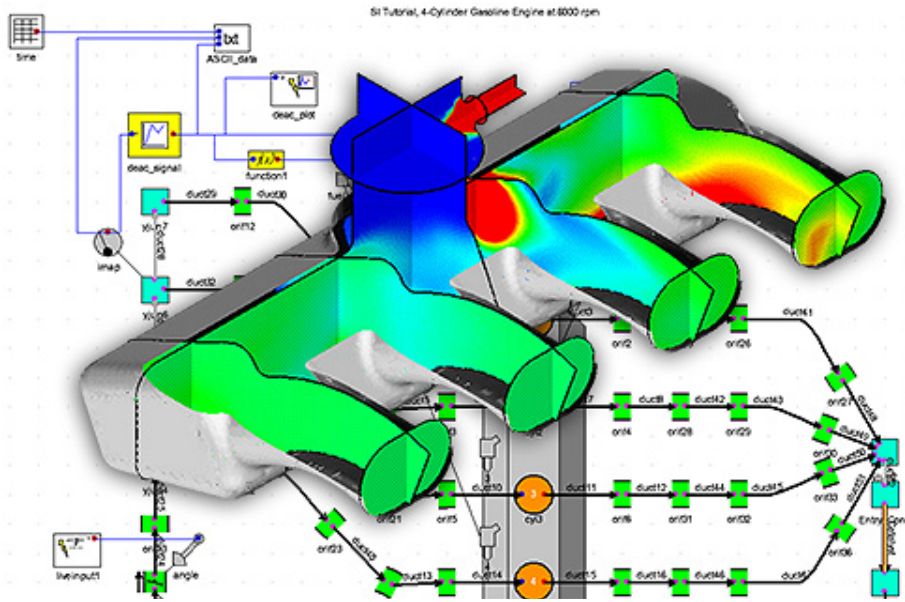
- more extensive circulatory networks
- fast-computing

Multi-domain modelling

- coupling of 3D domain reproducing specific vascular portions (e.g. surgery site) with the downstream circulation described by LPM or 1D model
- **closed-loop** approach to account for the mutual interaction between the two domains.

CFD allows an approximation of a real situation, dividing the physical problem domain (object) in smaller parts (elements or volumes) and solving each single part. If the division (mesh) is good, the results are an approximation, but very close to the reality.

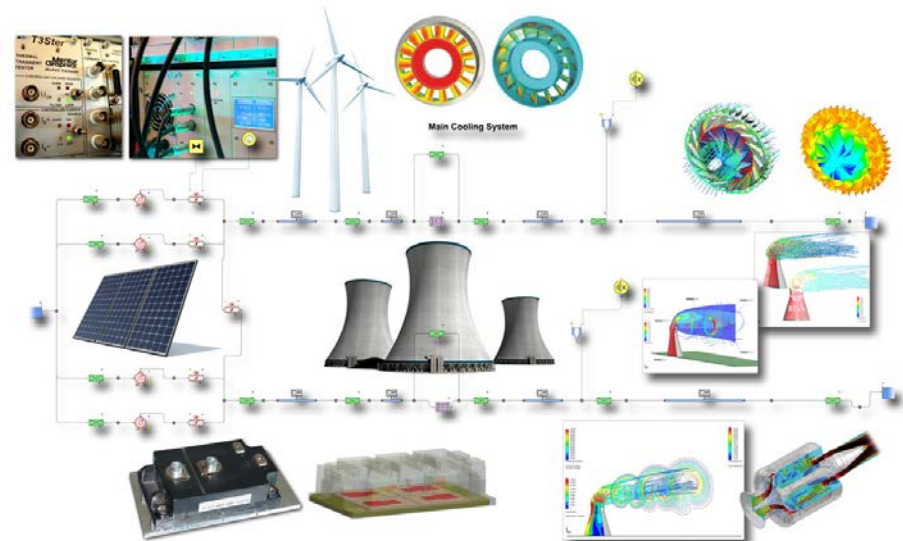




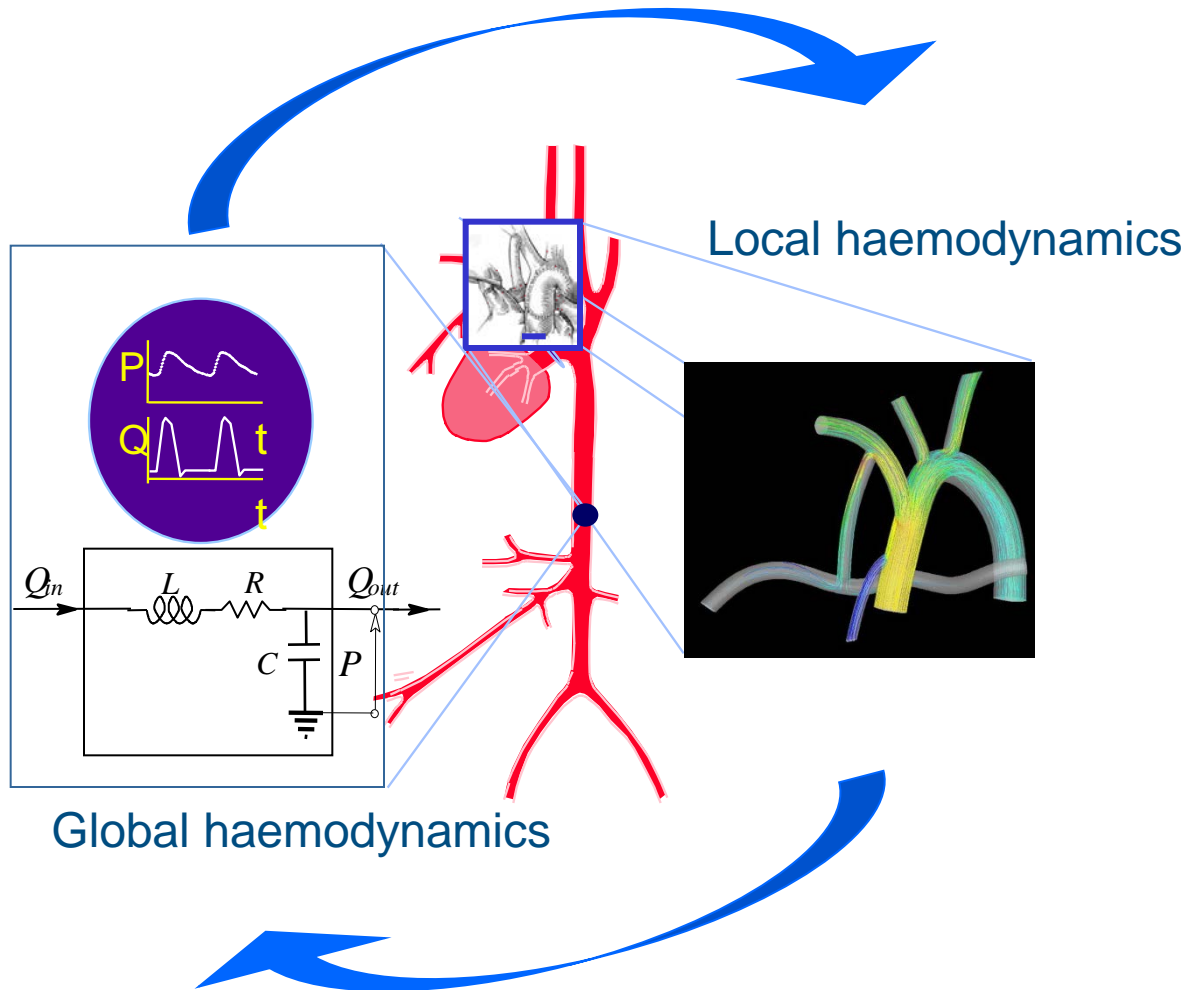
[from <http://xpsolutions.com/Software/XP2D/>]

[from <http://www.ricardo.com/en-GB/What-we-do/Software/Products/VECTIS/Coupled-1D3D-Analysis/>]

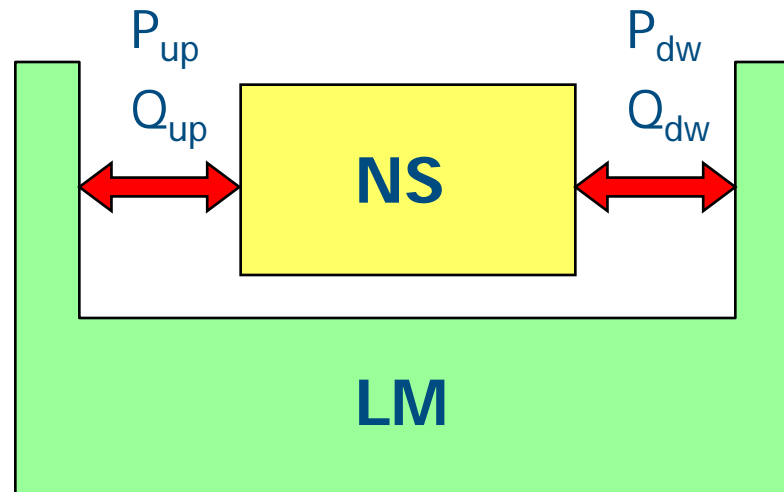
Multi-domain model approach already in use in the automotive industry (e.g. intake and exhaust runners), environmental planning (e.g. impact of surface flooding on an existing sewer network), power generation industry (e.g. wind plant design), etc.



[from <http://www.mentor.com/products/mechanical/flowmaster/flowmaster-process-power-energy/>]



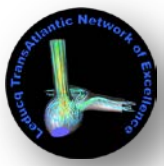
Partial differential equations (Navier-Stokes)



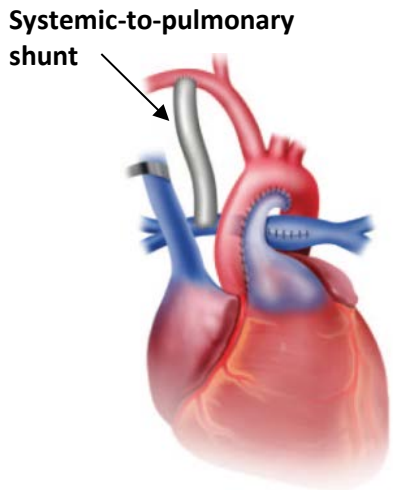
Ordinary differential equations (ODE)

Quarteroni et al. "Coupling between lumped and distributed models for blood flow problems." Computing and Visual Science 4, 111-124, 2001.

Introduction: single-ventricle congenital heart diseases

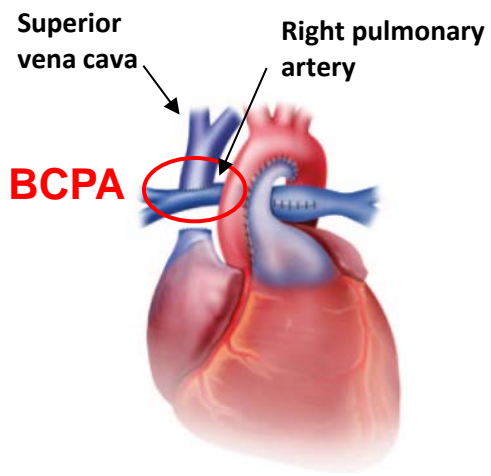


Stage 1



few days

Stage 2

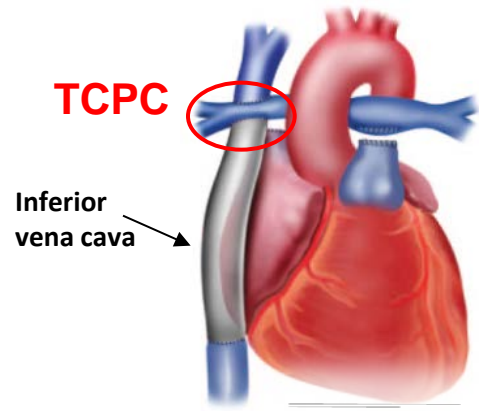


6 months

Bidirectional Cavo-Pulmonary Anastomosis

Hemi-Fontan

Stage 3



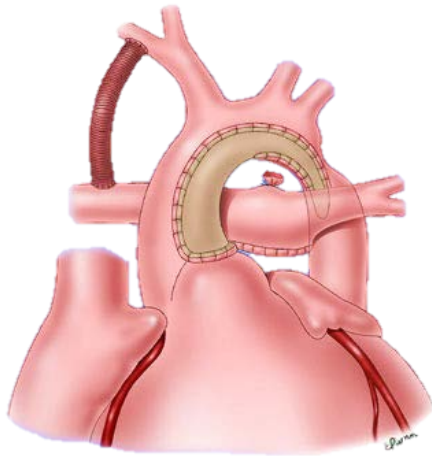
3-5 years

Total Cavo-Pulmonary Connection

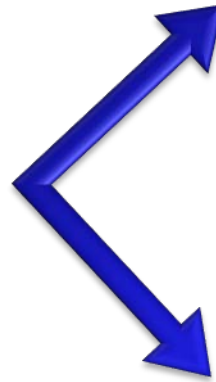
Y-Graft – Lateral tunnel - ECC

PRE-OPERATIVE

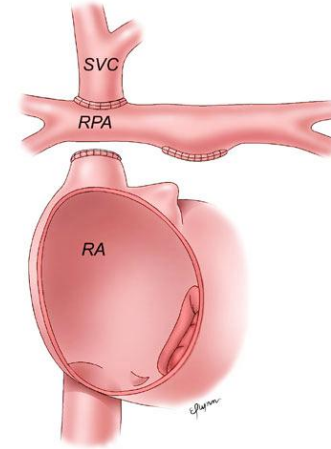
Stage 1



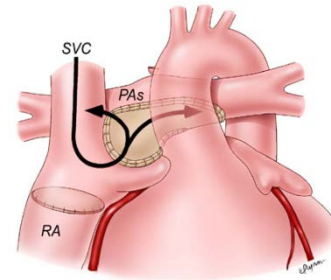
Stage 2
surgical
options



POST-OPERATIVE



Glenn



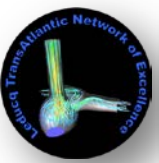
Hemi-Fontan

www.childrenshospital.org

Steps of a **virtual surgical planning**:

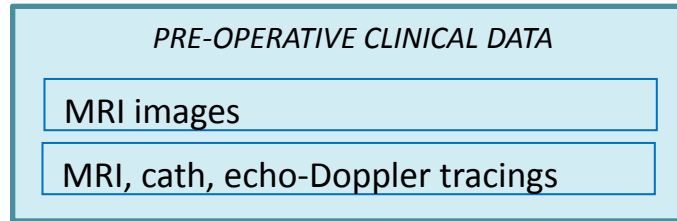
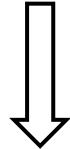
- implementation of a **pre-operative computational model** to reproduce the hemodynamics of the patient
- comparison of **different surgical options** through CFD analysis.

WORKFLOW



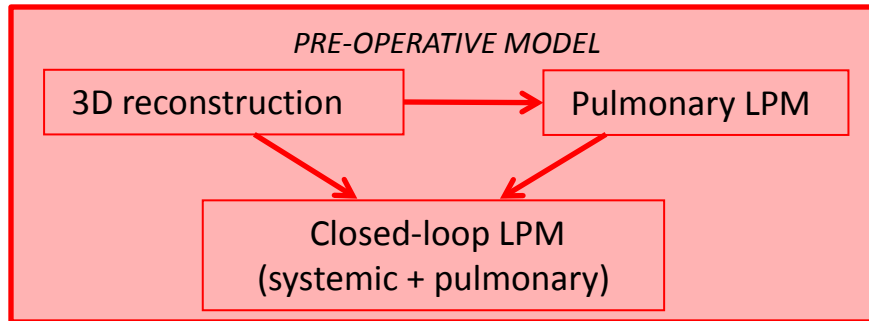
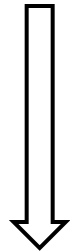
- MR images
- Selected pressures and flows

Step 1



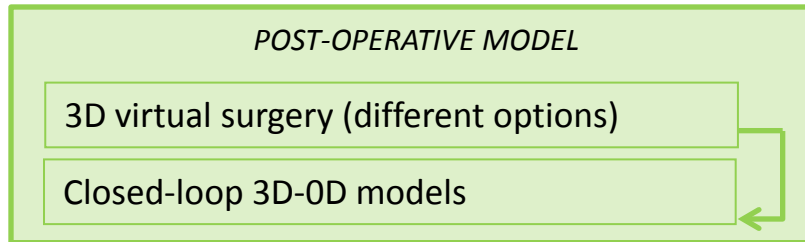
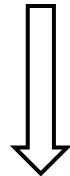
- 3D pre-op model
- Pre-op LPM

Step 2

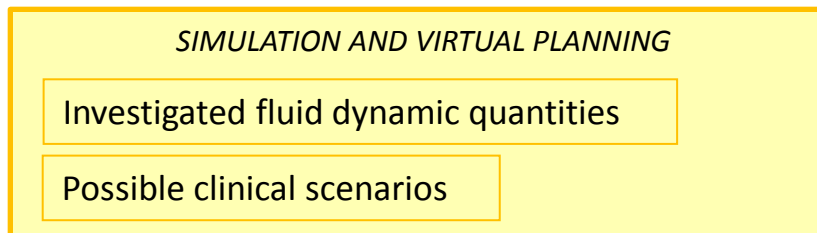


- Comparison
- Prediction

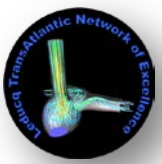
Step 3



Step 4

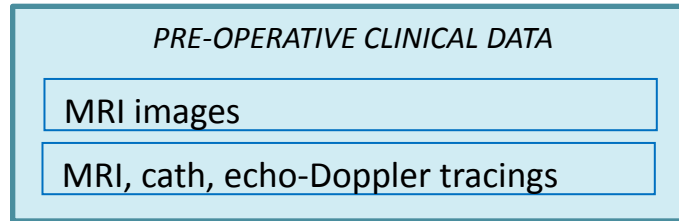
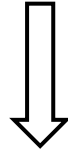


WORKFLOW



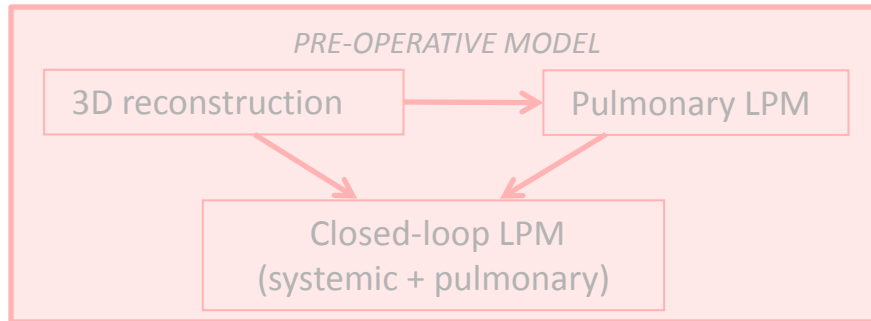
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Step 1



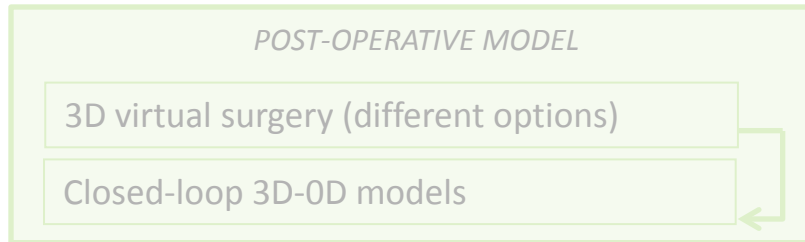
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Step 2

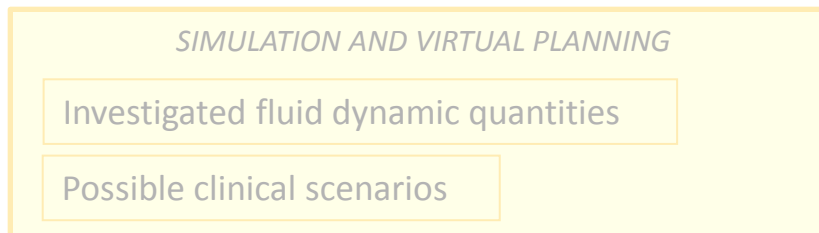


- Comparison
- Prediction

Step 3

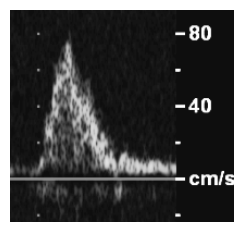


Step 4

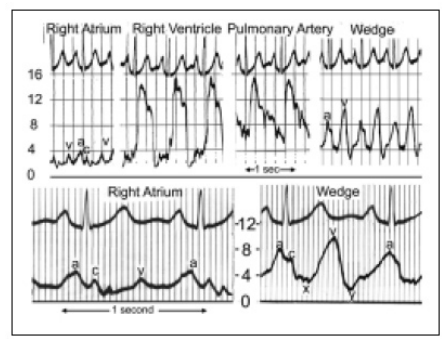
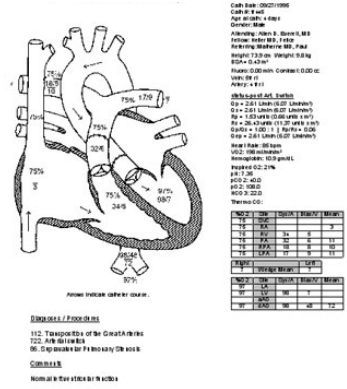


STEP 1: Pre-operative clinical data

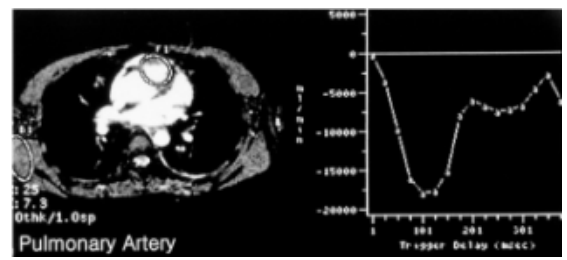
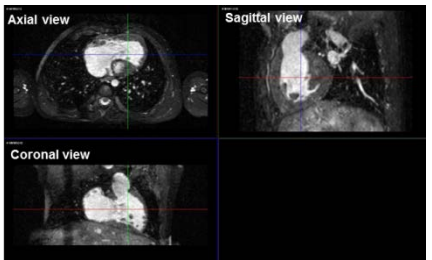
Doppler acquisition



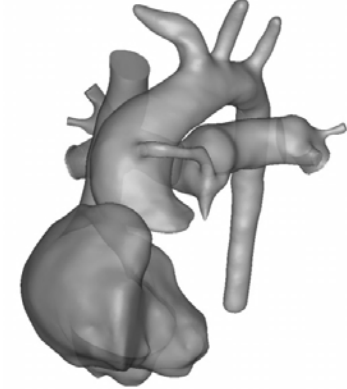
Catheterization



MR imaging and flows



Three-dimensional MR data reconstruction

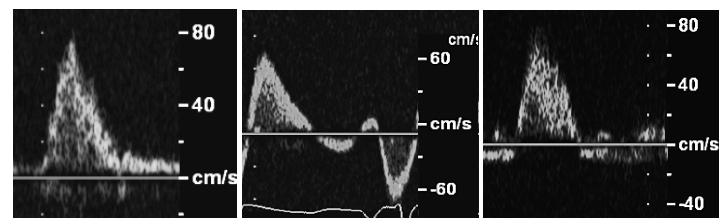


STEP 1: Pre-operative clinical data



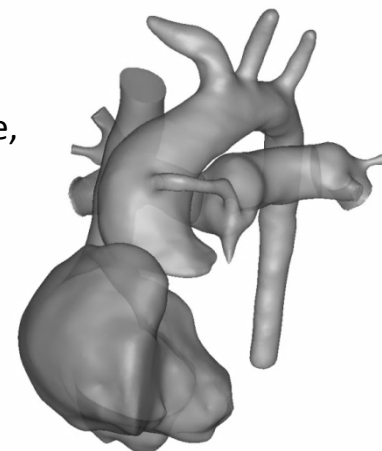
- ✓ 6 months-old infant (weight 6.9 kg, BSA 0.34 m²)
- ✓ Hypoplastic right heart syndrome + pulmonary atresia
- ✓ 3.5 mm central shunt (from AoA to MPA) surgically placed on day of life #5

Doppler acquisition (5 weeks prior to surgery, under sedation)
Echocardiography system (iE33, Philips, Best, Netherlands)



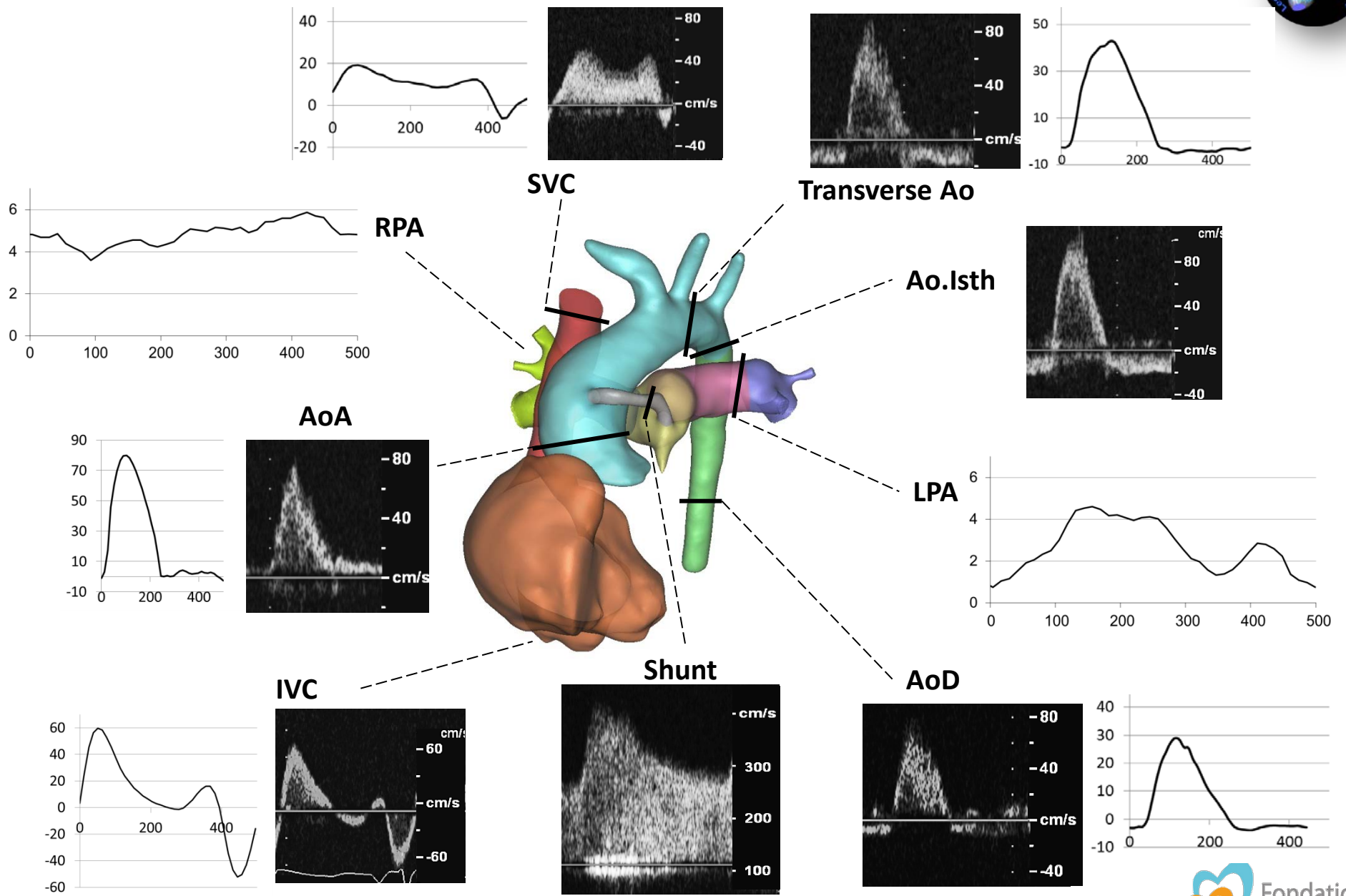
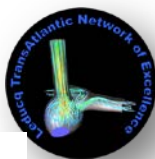
Catheterization (under sedation, 3 days before the surgery)
Biplane fluoroscopy suite (Toshiba America Med. Syst., Inc., CA, or Siemens Med. Solutions, USA, Inc. PA).

MR imaging (under general anesthesia immediately prior to surgery)
1.5 T scanner (Philips Intera Achieva, Best, Netherlands).
Imaging parameters: 4.4/2.3 (repetition time msec/echo time msec), 12° flip angle, 1.3–1.5-mm section thickness, 256 × 512 matrix, 400–500-mm field of view, one breath hold, one signal acquired, no electrocardiographic gating.

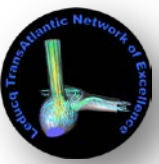


Three-dimensional MR data reconstruction
Mimics software (Materialise NV, Leuven, Belgium).
Image elaboration for each patient's MR data took 2–3 hours.

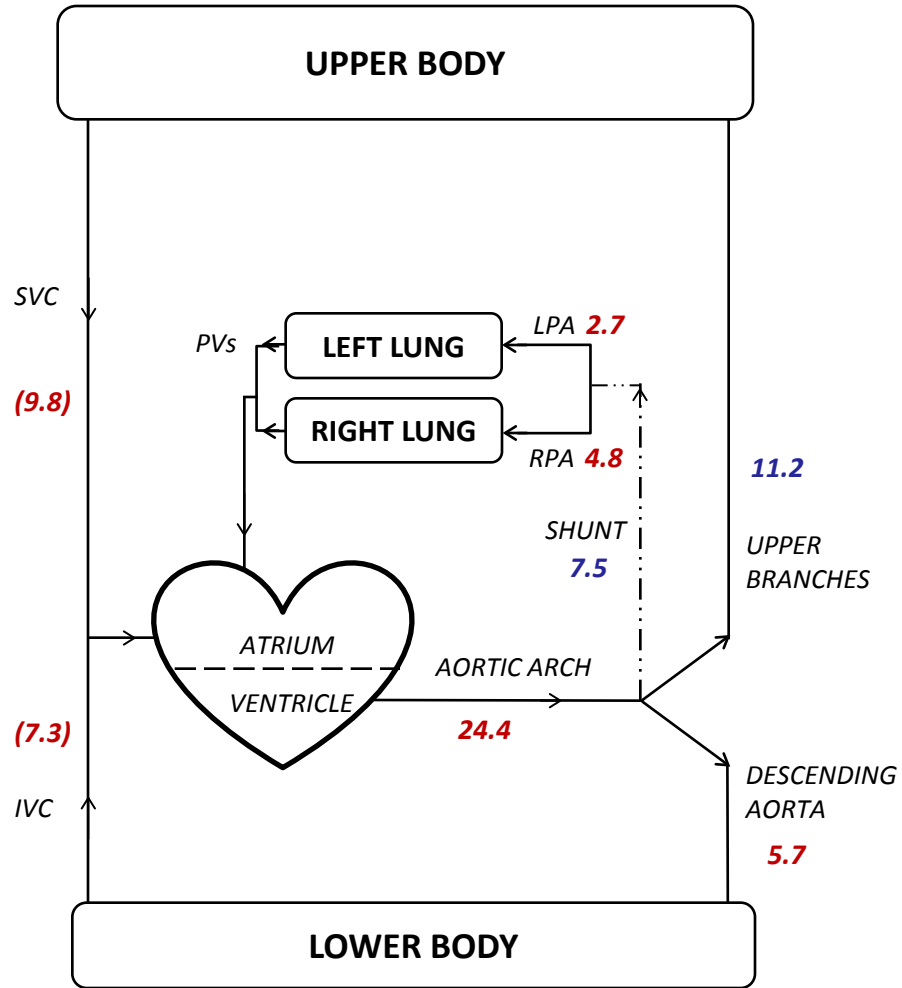
STEP 1: Pre-operative clinical MRI and Doppler flows



STEP 1: Pre-operative clinical data



[mmHg]	Pressures
P_{SV}	6 / 103 / 54
P_{SA}	5
P_{PA}	13
P_{SVC}	9
P_{DAo}	43
[ml]	Volumes
EDV	22.6
ESV	9.6

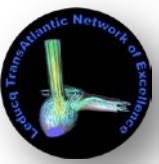


(MEASURED FLOWS – NOT USED)

MEASURED FLOWS [ml/s]

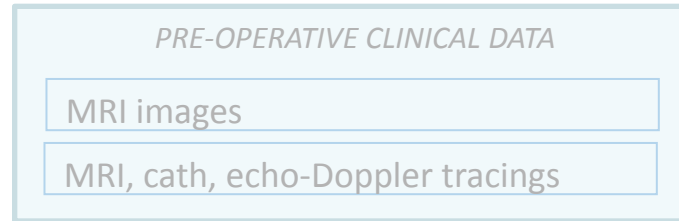
CALCULATED FLOWS

WORKFLOW



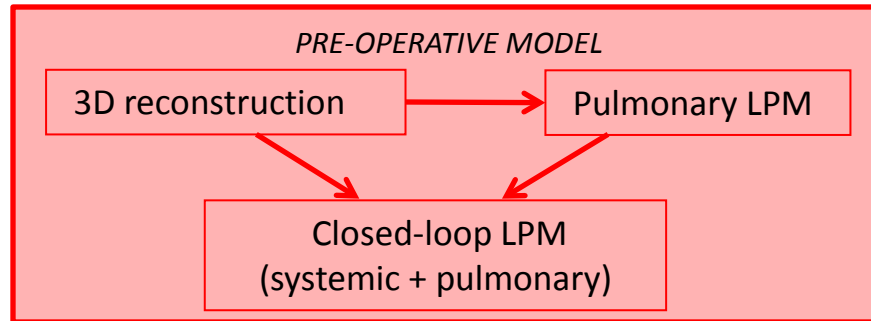
- MR images
- Selected pressures and flows

Step 1



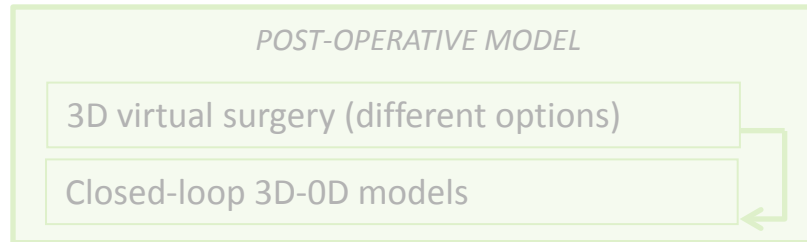
- 3D pre-op model
- Pre-op LPM

Step 2

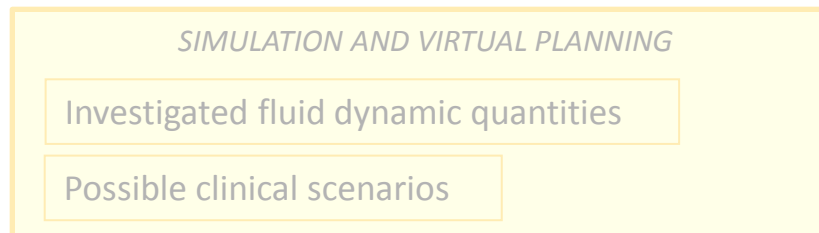


- Comparison
- Prediction

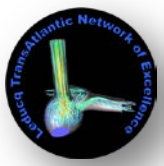
Step 3



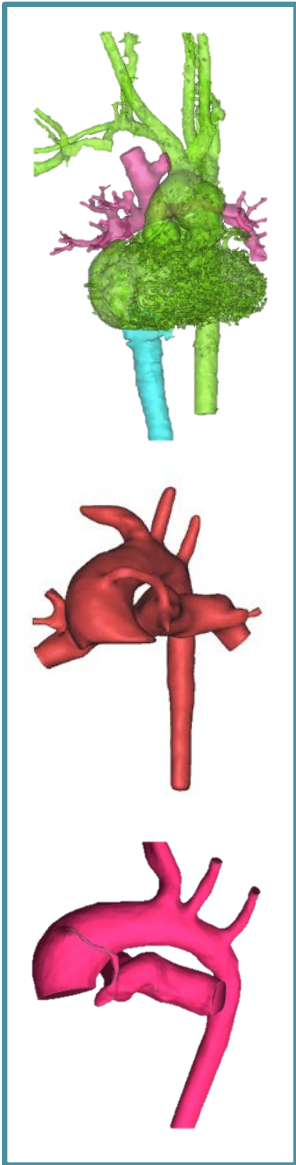
Step 4



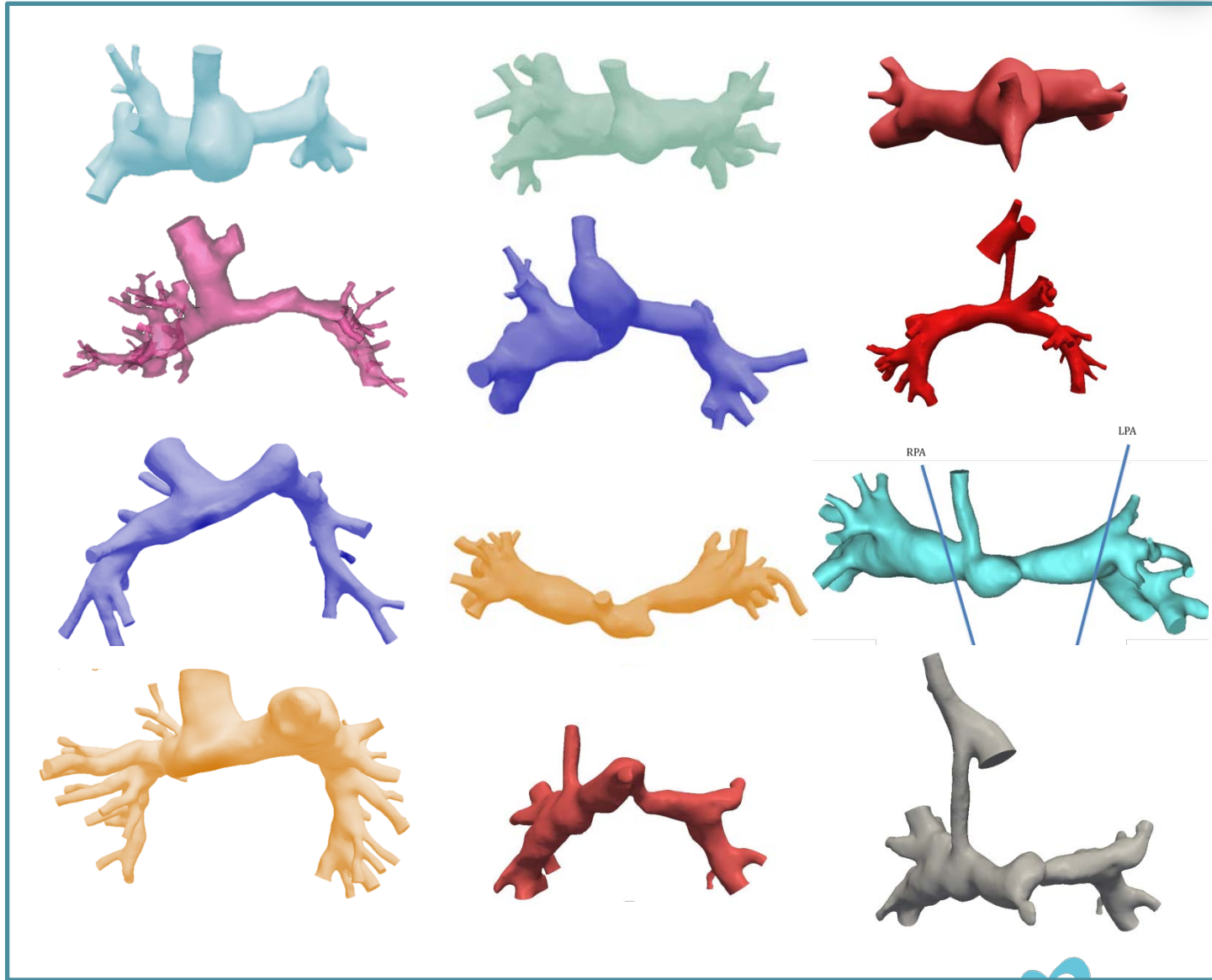
STEP 2: Pre-operative 3D reconstruction



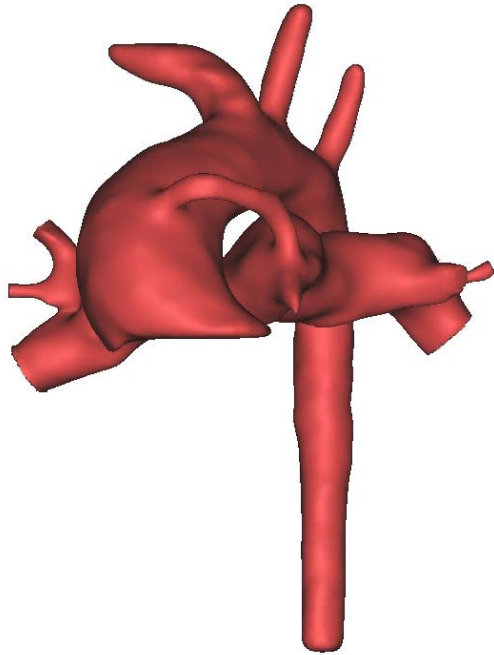
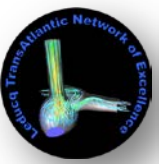
Whole geometry reconstruction



Selection of the sub-model of the pulmonary arterial vasculature



STEP 2: Pre-operative 3D reconstruction



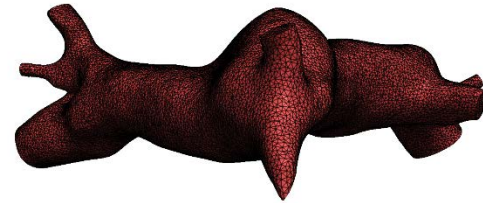
Whole geometry reconstruction



Selection of the sub-model of the pulmonary arterial vasculature

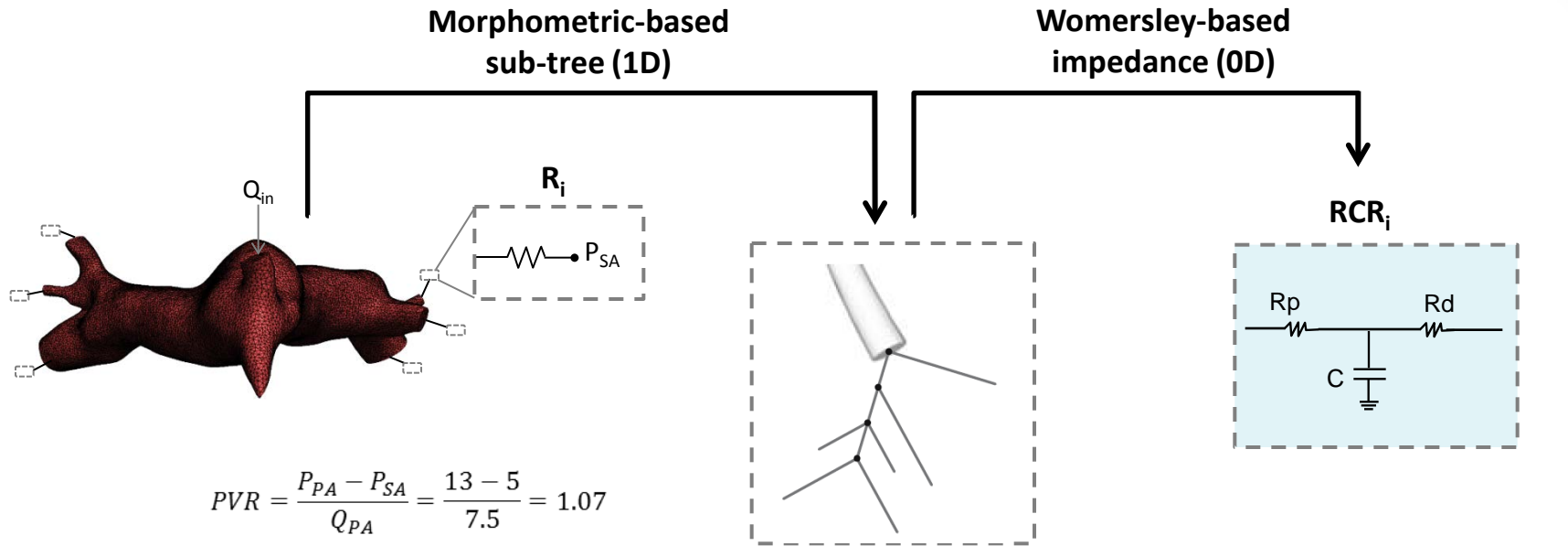


MESHSIM
(Simmetrix, Inc., NY)



Volume meshing

STEP 2: Pre-operative pulmonary LPM - morphometric approach



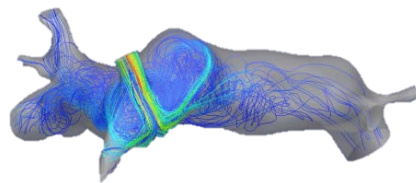
$$PVR = \frac{P_{PA} - P_{SA}}{Q_{PA}} = \frac{13 - 5}{7.5} = 1.07$$

R_i of each i -th outlet based on:

- inflow Q_{in}
- flow split between right and left lungs
- ΔP between 3D inlet and single atrium SA
- size of each outlet branch $Q_i \propto S_i^\alpha$

- The sub-tree with the impedance spectrum closest to R_i is selected.
- R_p , C , R_d are given by least-squares fit of the impedance spectrum

Iterative simulations until convergence



Troianowski et al., 2011 J. Biomech. Eng.
Spilker et al., 2007 Ann. Biomed. Eng.

STEP 2: Pre-operative closed-loop LPM

Setting of the parameters

- $HR = 120$ bpm
- $BSA = 0.34$ m²
- Vascular resistances [mmHg*s/ml]

$$UBSVR = \frac{P_{Ao} - P_{SA}}{Q_{UBA}} = \frac{43 - 5}{11.2} = 3.39$$

$$LBSVR = \frac{P_{Ao} - P_{SA}}{Q_{THAO}} = \frac{43 - 5}{5.7} = 6.67$$

- Pulmonary RCRs provided by morphometric approach

Shunt

Operating point: $dP = 43 - 13 = 30$ mmHg, $Q_{SH} = 7.5$ ml/s

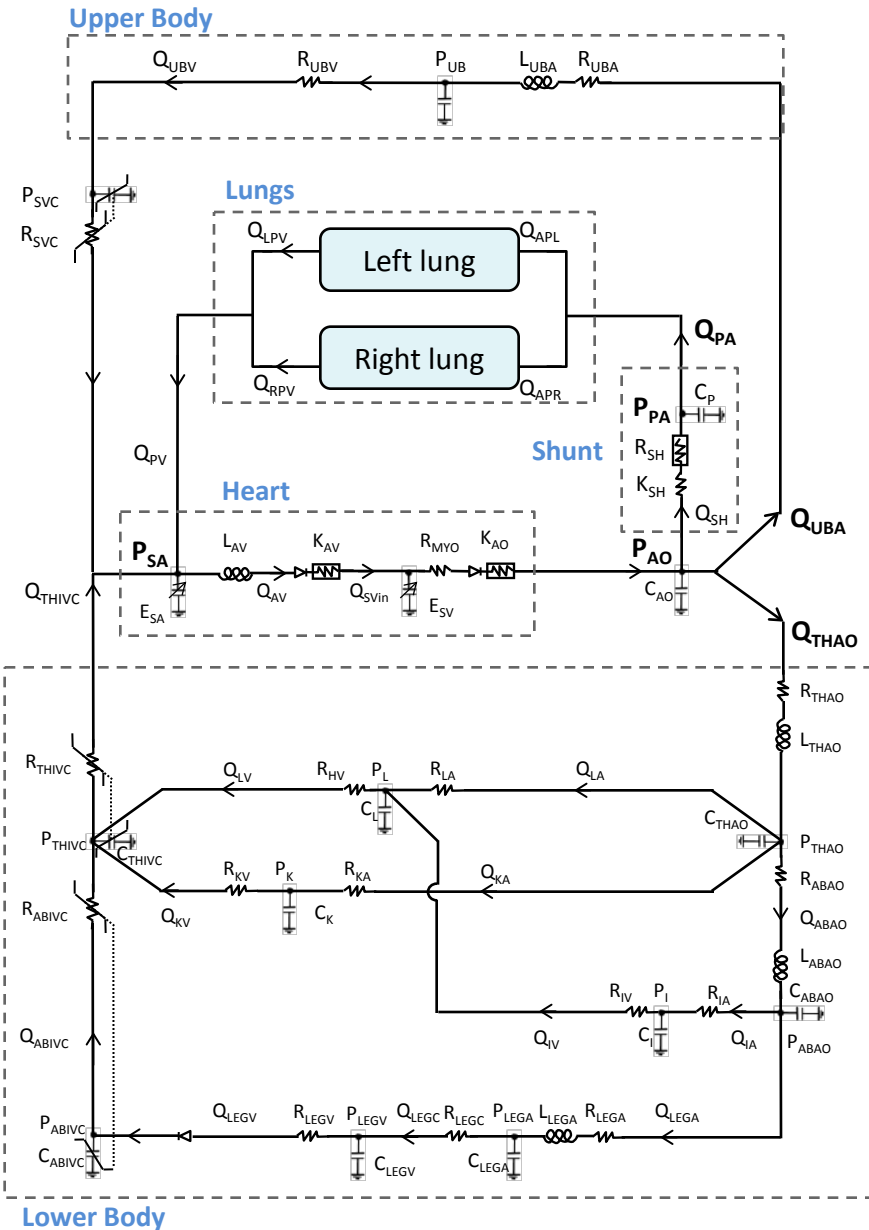
$$\text{Relation: } dP = R_{SH} Q_{SH} + K_{SH} Q_{SH}^2$$

Migliavacca et al., 2001, Am J Physiol Heart Circ Physiol

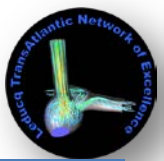
- Respiratory effects were not included

- Single values of resistance and compliance vary depending on the BSA

Snyder, Rideout, 1969, IEEE Trans Bio-Med Eng



STEP 2: Pre-operative closed-loop LPM - Results

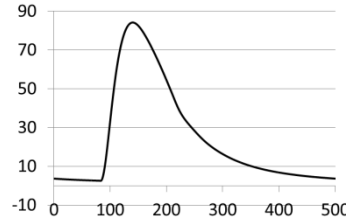
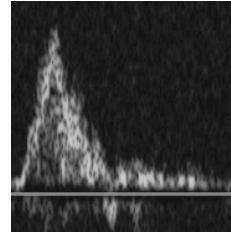
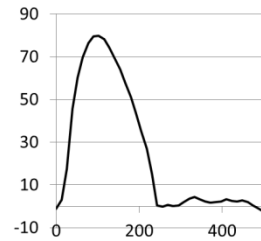


MRI

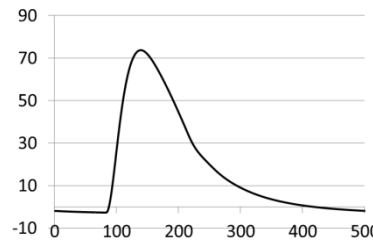
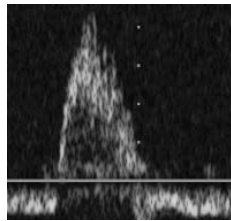
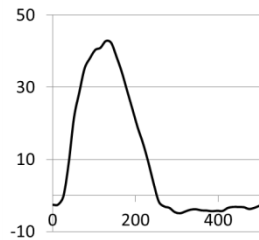
DOPPLER

LPM

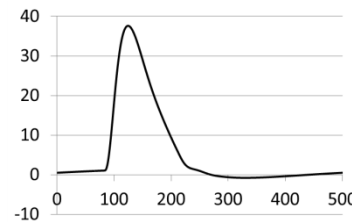
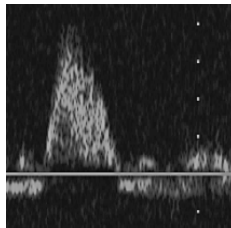
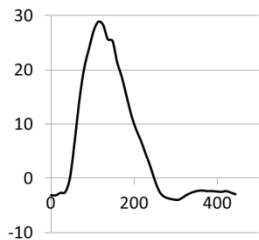
A.Ao



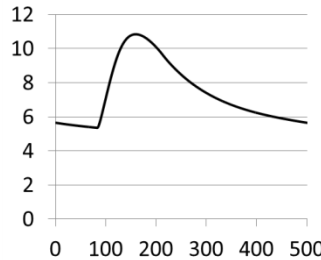
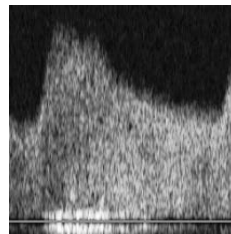
TransAo



D.Ao



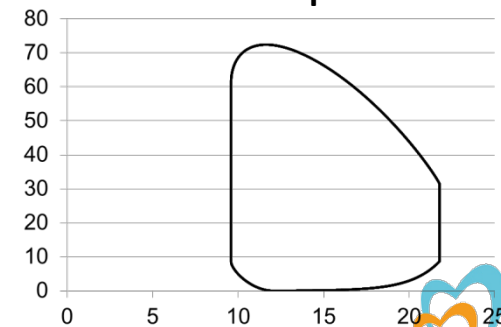
Shunt



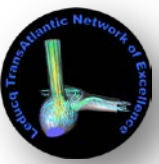
[ml/s]	Clinical mean values	LPM
Q_{UB}	11.2	11.3
Q_{LB}	5.7	5.7
Q_{LPA}	2.7	2.8
Q_{RPA}	4.8	4.8
CO	24.4	24.4

[mmHg]	Reference clinical data	LPM
P_{SV}	6 / 103 / 54	0 / 72 / 25
P_{SA}	5	6.8
P_{PA}	13	14.7
P_{SVC}	9	7.9
P_{DAo}	43	43.8
[ml]	Clinical mean values	LPM
EDV	22.6	21.8
ESV	9.6	9.6

PV Loop



STEP 2: Pre-operative closed-loop LPM - Results

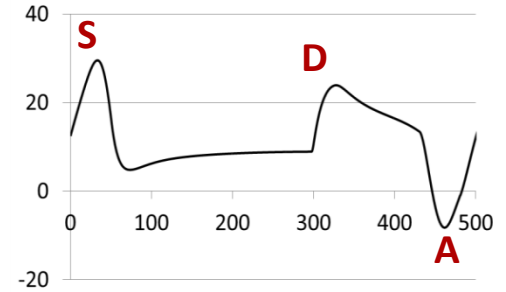
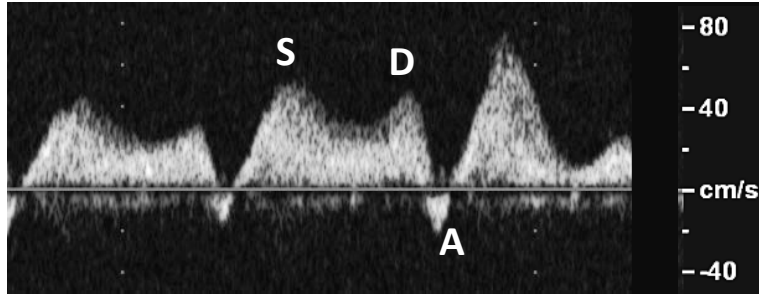
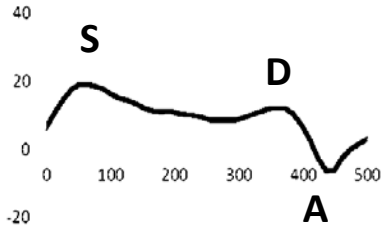


MRI

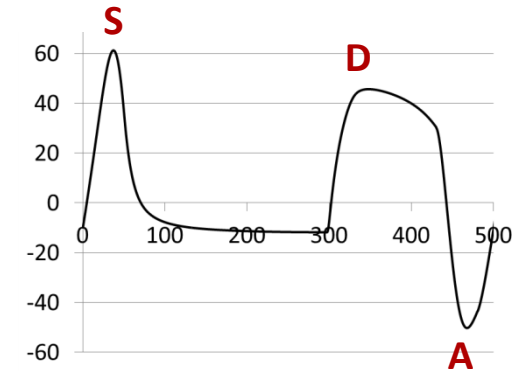
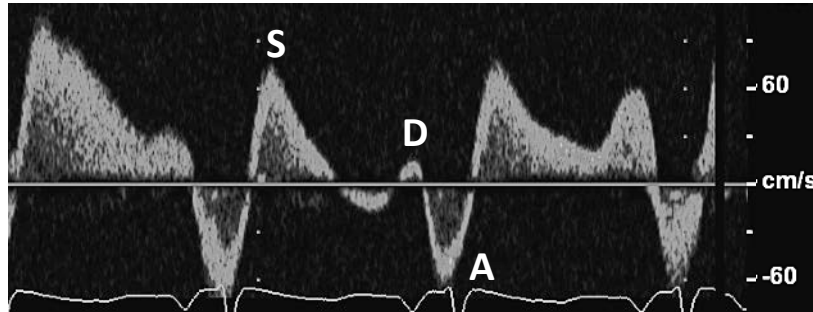
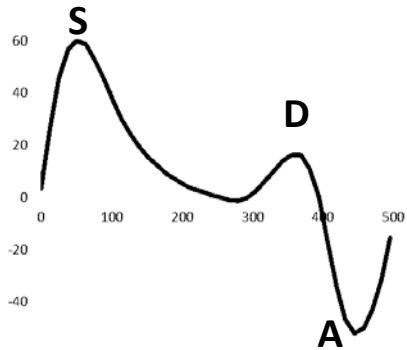
DOPPLER

LPM

SVC

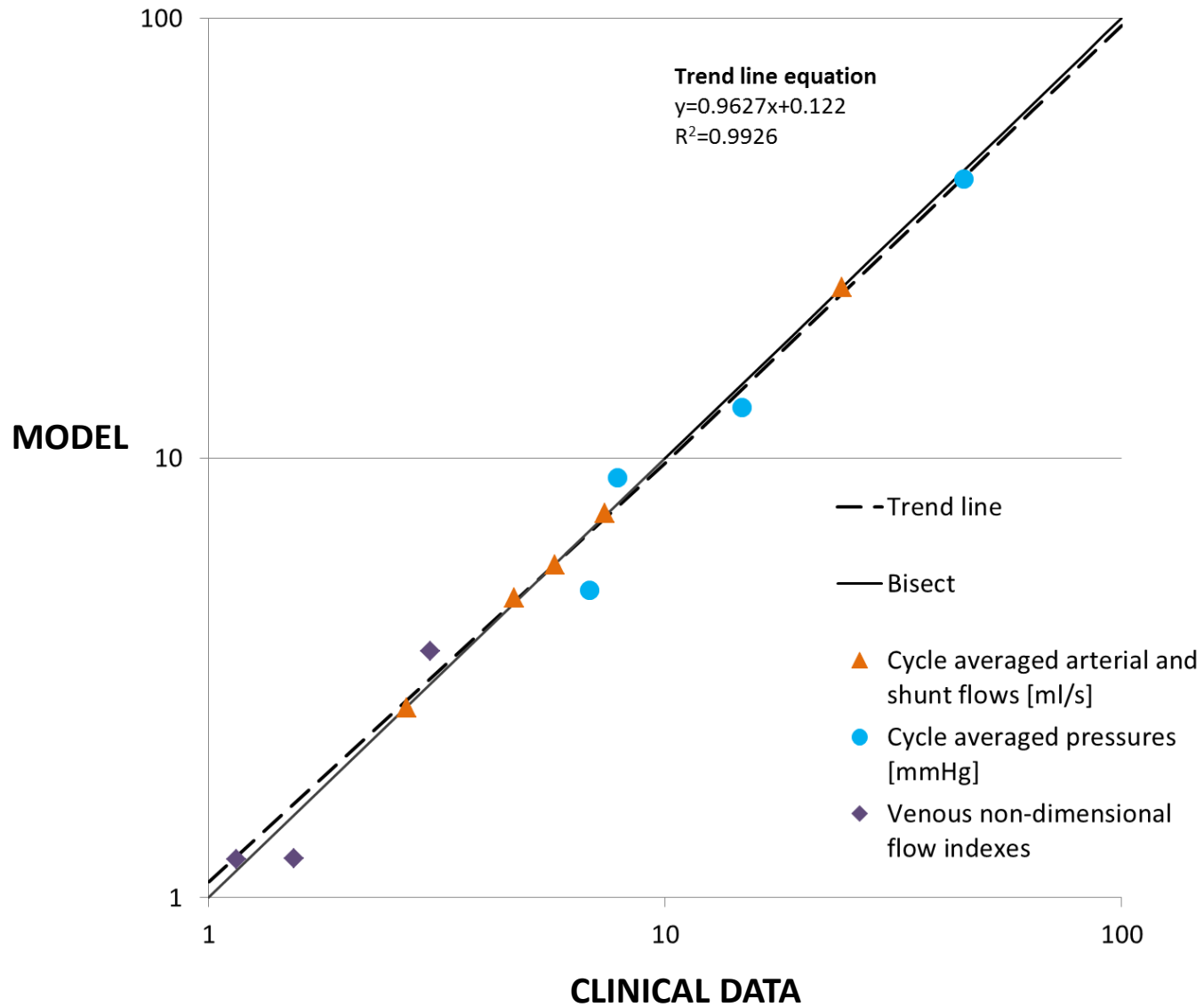
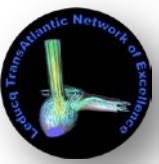


IVC

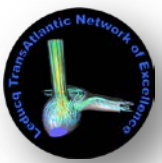


	MRI	LPM
S/D SVC	1,54	1,49
S/A SVC	-3,06	-3,05
S/D IVC	3,75	2,33
S/A IVC	-1,15	-0,95

STEP 2: Pre-operative closed-loop LPM - Results

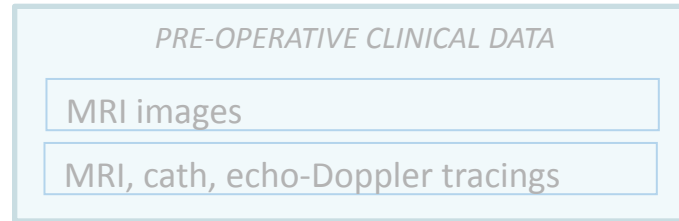


WORKFLOW



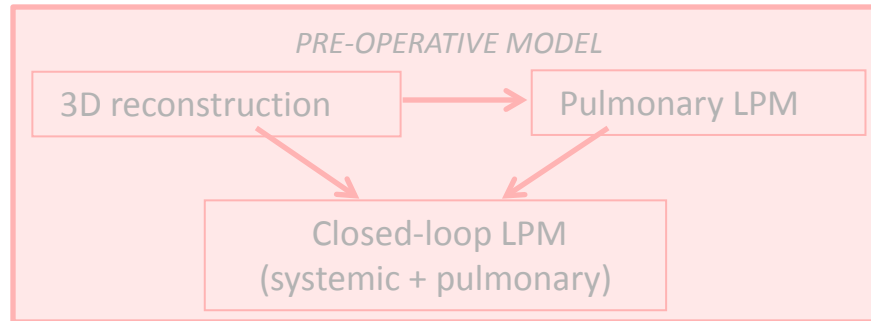
- MR images
- Selected pressures and flows

Step 1



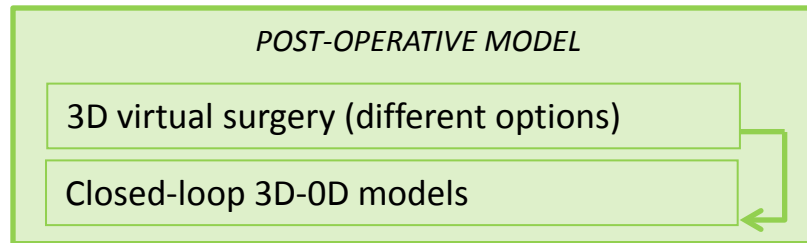
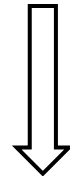
- 3D pre-op model
- Pre-op LPM

Step 2

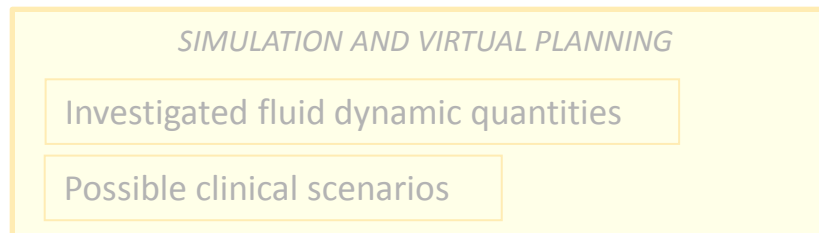


- Comparison
- Prediction

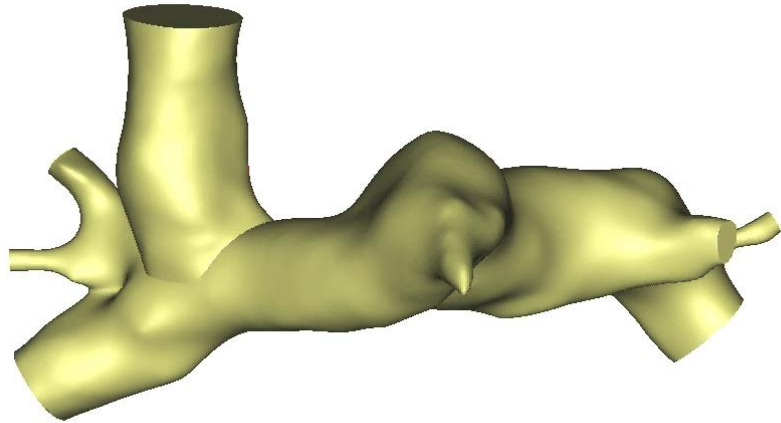
Step 3



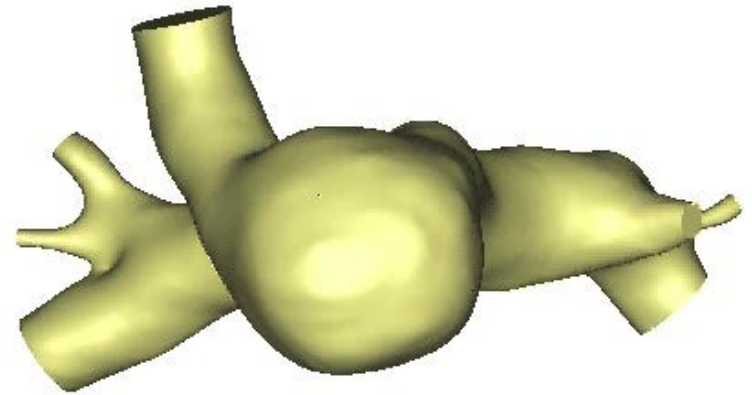
Step 4



Different options:

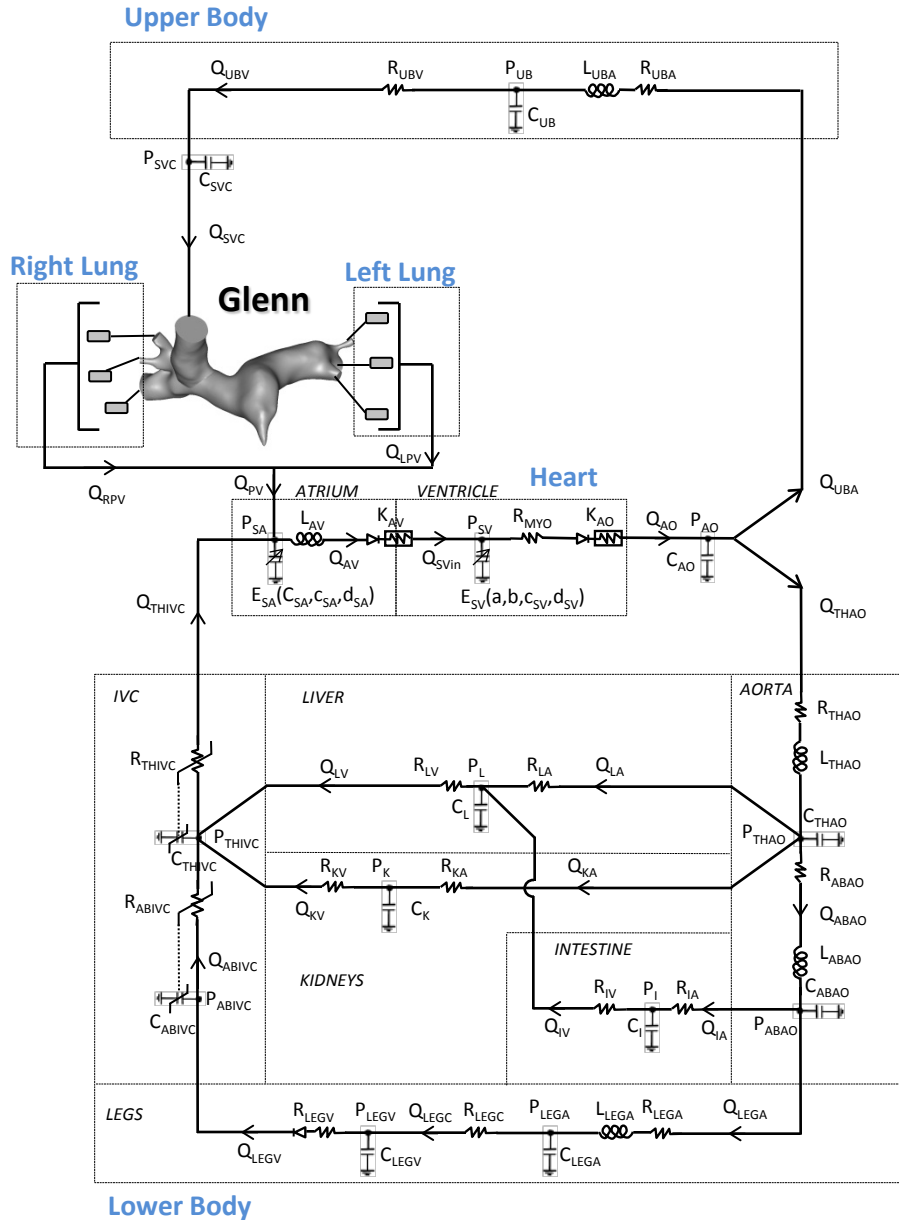
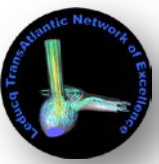


Glenn

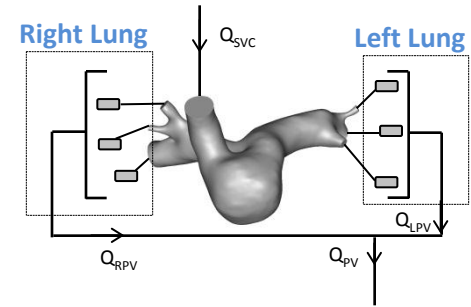


hemi-Fontan

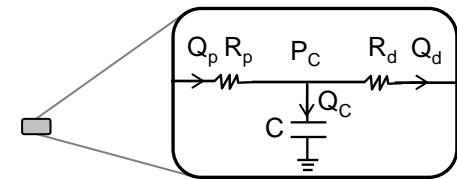
STEP 3: Post-operative model – closed-loop 3D-0D models



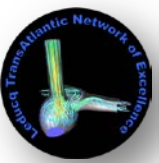
Hemi-Fontan



Pulmonary RCR blocks

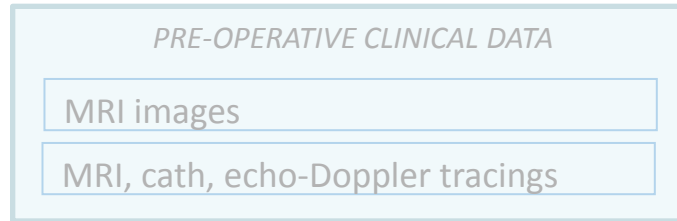


WORKFLOW



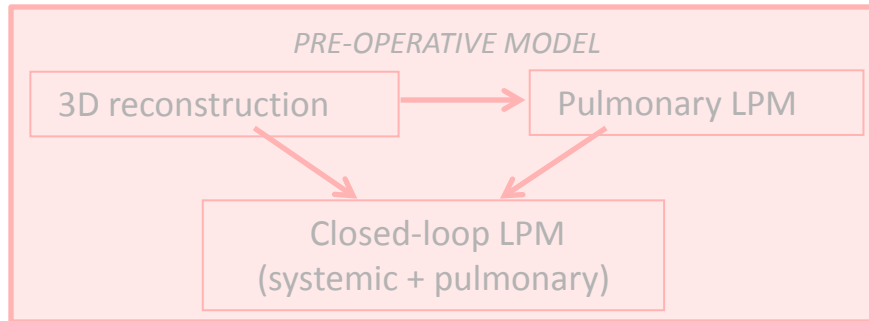
- MR images
- Selected pressures and flows

Step 1



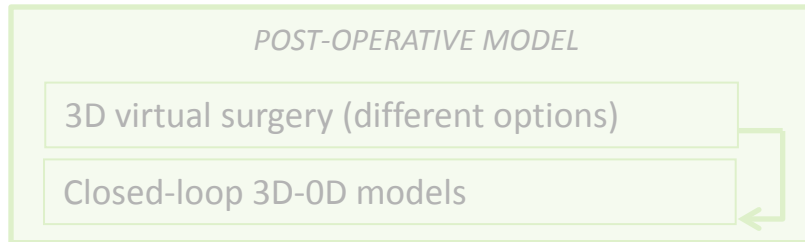
- 3D pre-op model
- Pre-op LPM

Step 2

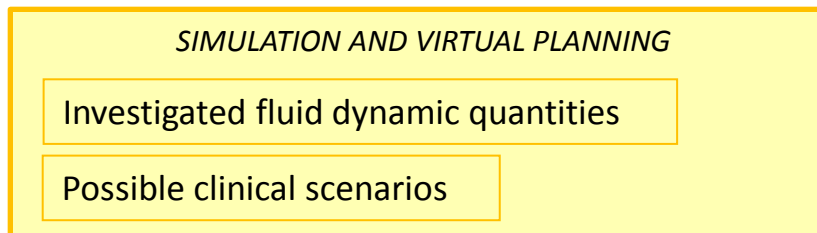


- Comparison
- Prediction

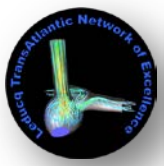
Step 3



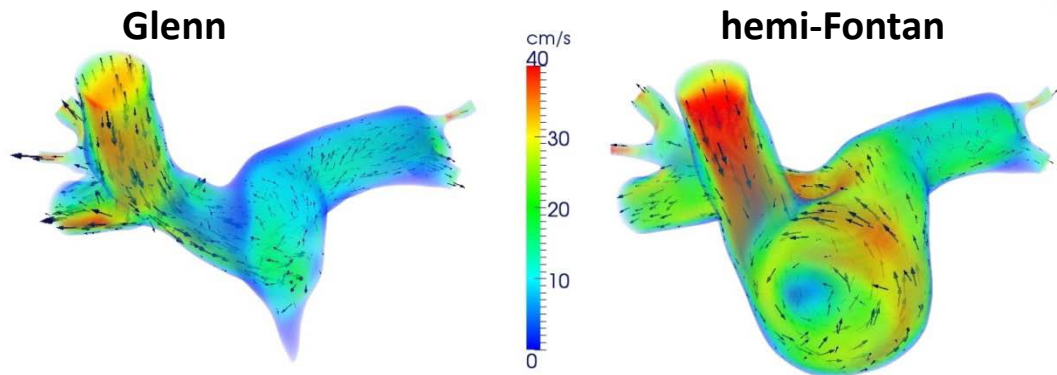
Step 4



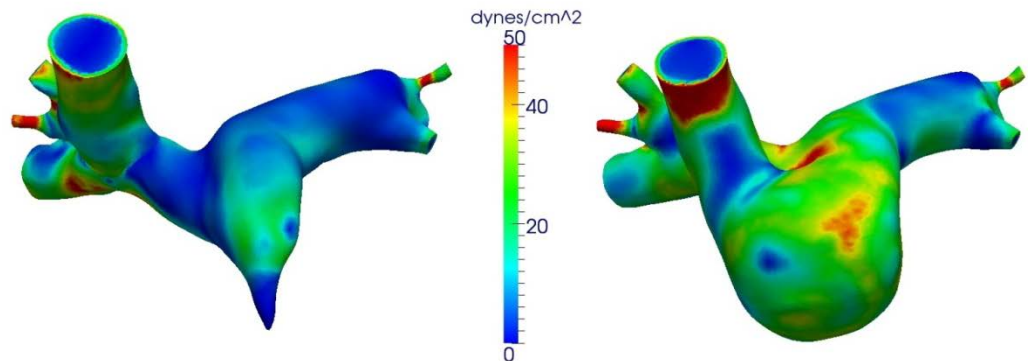
STEP 3: Post-operative model – Simulation results



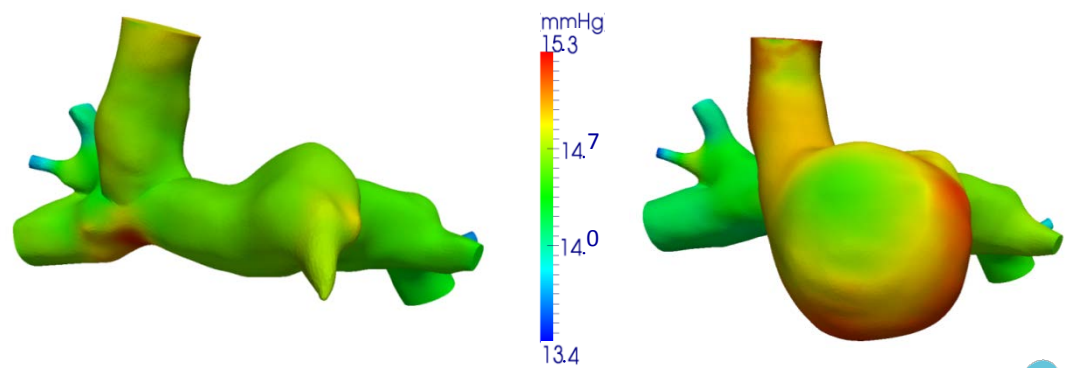
Velocities at peak flow



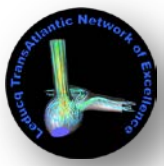
Time-averaged wall shear stress (WSS)



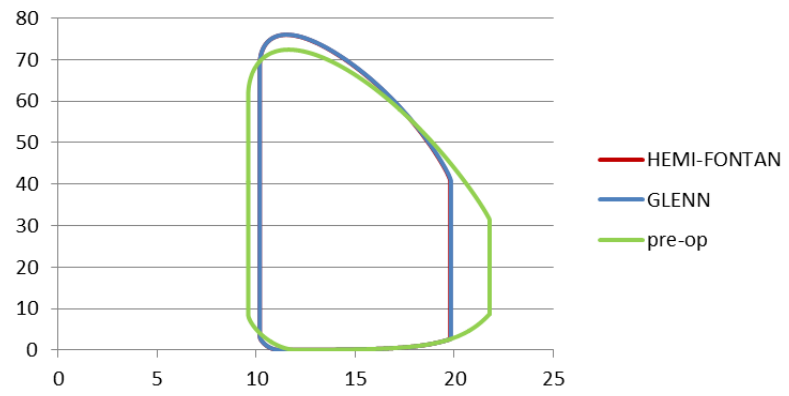
Time-averaged pressures



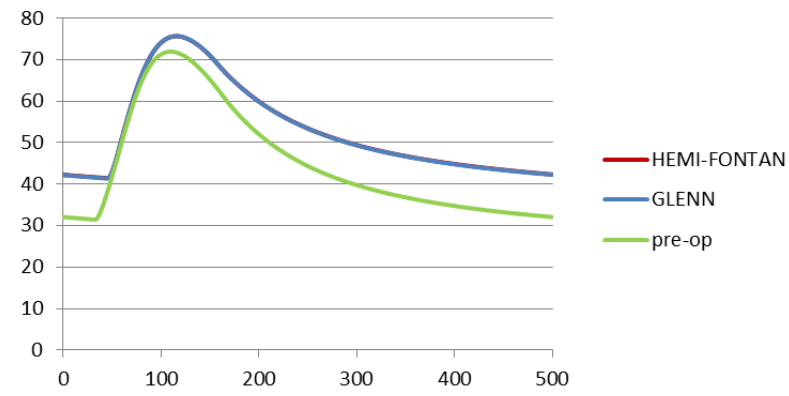
STEP 3: Post-operative model – Simulation results



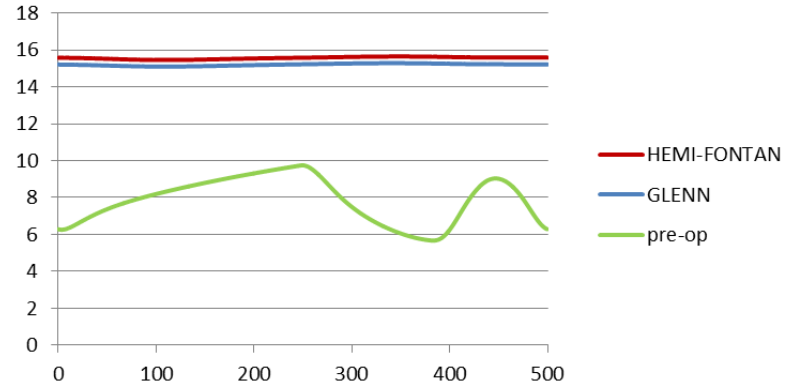
P-V loop



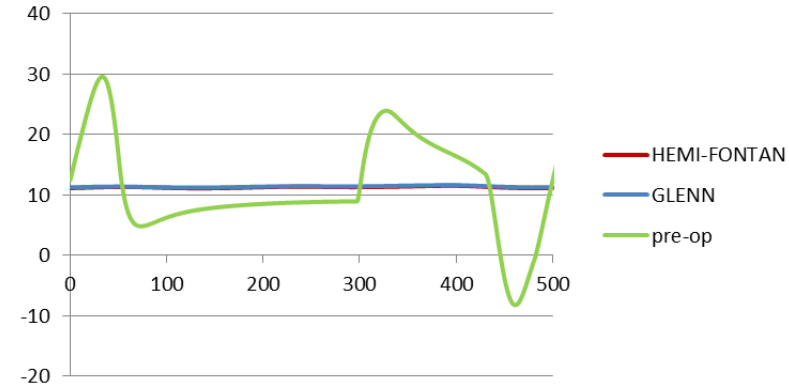
Aortic pressure



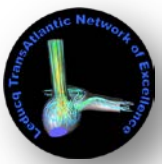
SVC pressure



SVC flow rate



STEP 3: Post-operative model – Simulation results



Investigated fluid dynamic quantities	Glenn	Hemi-Fontan
Q_{SVC} (ml/s)	11.4	11.3
Q_{IVC} (ml/s)	7.87	7.89
Q_{LPA} (ml/s)	4.17	4.21
Q_{RPA} (ml/s)	7.21	7.07
P_{SVC} (mmHg)	15.1	15.4
P_{Ao} (mmHg)	53.1	53.1
P_{SA} (mmHg)	2.48	2.43
Power Loss-- Surgical Junction (mW)	0.61	1.26
Efficiency-- Surgical Junction	0.97	0.95
Ventricular power (mW)	166	166

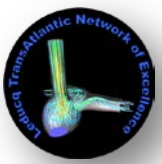
The workflow

- constant interactions among clinicians and engineers to:
 - collect the patient's clinical data
 - select the data to be used in the modeling process
 - build a preoperative patient-specific model that reproduced the patient
 - simulate different postoperative surgical options
 - compare the local and global hemodynamic results

Not shown

- Different postoperative scenarios (e.g. agitation, exercise) have been simulated

Acknowledgements



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UCSD, CA, USA

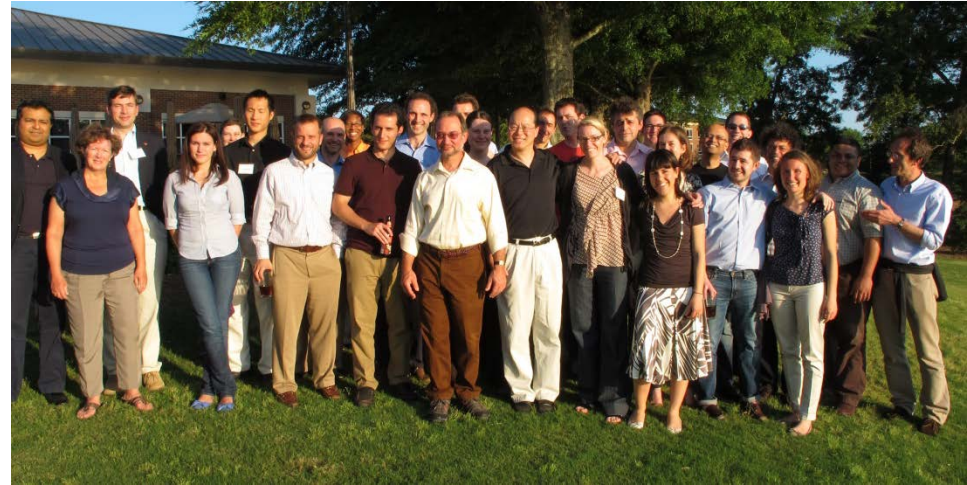
INRIA Paris-Rocquencourt, Le Chesnay, France

UCL Institute of Cardiovascular Science, London, UK

University of Michigan, Ann Arbor, MI, USA

Medical University of South Carolina, Charleston, SC, USA

Stanford University, Stanford, CA, USA



“Multi-scale Modeling of Single Ventricle Hearts for Clinical Decision Support” Transatlantic Project

<http://modelingventricle.clemson.edu>

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